S & M 1574

Characterization and Optimization of Thermally Grown Iridium Oxide and Its Application to pH Sensors

Chindanai Ratanaporncharoen,¹ Miyuki Tabata,¹ Natthapol Watanagool,² Tatsuro Goda,¹ Akira Matsumoto,¹ Mana Sriyudthsak,² and Yuji Miyahara^{1*}

¹Institute of Biomaterials and Bioengineering, Tokyo Medical and Dental University, Tokyo 101-0062, Japan ²Department of Electrical Engineering, Chulalongkorn University, Bangkok 10330, Thailand

(Received August 31, 2017; accepted March 28, 2018)

Keywords: iridium oxide, pH microsensor

In this study, we evaluate the thermal oxidization methods of iridium to simplify the fabrication of Ir/IrOx pH microsensors. Iridium oxide (IrOx) is a typical pH-sensing material. Specifically, three parameters of the previously reported "carbonate-melt" method are modified, namely, the oxidization temperature, oxidization time, and annealing process after oxidization. Then, we compare the characteristics of the fabricated sensors (i.e., the initial pH responsivity, time required to reach the steady state, and potential drift). The pH response depends on oxidization temperature and time.

1. Introduction

Proton kinetics is the main indicator for understanding numerous biological and chemical reactions.⁽¹⁾ In the field of biosensors, pH sensors are essential tools as transducers because many reactions in biomechanisms are pH-dependent. Moreover, pH is also an indicator for the reaction rate of an electron transfer by-product.^(2–4) As a conventional sensor to measure pH *in vitro*, glass-type pH electrodes have been used for decades owing to their simplicity. Many clinical studies have been conducted with glass-type electrodes,^(5,6) but some applications such as *in vivo* studies are incompatible owing to the properties of glass-type electrodes, such as brittleness and size limitations. To overcome these problems, other miniaturized electrodes such as ion-sensitive field-effect transistors (ISFETs)⁽⁷⁾ and optical pH sensors^(8,9) have been employed. Although the pH sensing system with ISFET has attracted attention owing to the small sensing area and fast response, previous studies have revealed that temperature, hysteresis, and drift impact the measurement accuracy.^(10–12) Additionally, the photosensing system in optical pH sensors is limited because more precise instrumentation directly alters the costs.

Generally, metal oxides are excellent proton-sensitive materials. Iridium oxide (IrOx) is a well-known pH-sensitive material. Its properties include proton selectivity, a nearly Nernstian

^{*}Corresponding author: e-mail: miyahara.bsr@tmd.ac.jp http://dx.doi.org/10.18494/SAM.2018.1733

pH response, a fast response time, long-term durability, shape reforming, and nontoxicity of the material.^(13,14) These features suggest that IrOx is compatible with clinical studies. Many fabrication techniques have been proposed to improve the pH selectivity. Examples include sputtering deposition,⁽¹⁵⁾ electrochemical deposition,^(16–18) and thermal oxidization.⁽¹⁹⁾ Other studies have applied IrOx in the pH sensing of organisms.^(20,21) In particular, thermal oxidization is stable and durable for long-term usage.

The carbonate-melt method reported by Yao *et al.* shows a promising pH responsivity and fast response times.⁽¹⁹⁾ In practice, time is necessary for the sensor to obtain stable potential response data in the steady state after the oxidization process. Moreover, some of the parameters in the fabrication process can be improved.

In this study, we investigated the carbonate-melt⁽¹⁹⁾ fabrication method to improve sensor performance. Since the thickness of the oxide layer affects the robustness of pH measurements, we systematically examined the effect of three parameters in the fabrication process: oxidization temperature, oxidization time, and annealing process after oxidization. Each parameter was separately varied and the electrochemical characteristics of the pH sensor were evaluated in terms of pH responsivity, drift potential at different pH values, and the time required to achieve a steady state. Compared with conventional methods, the modified method reduced the fabrication time, decreased the drift potential, and reduced the time required to reach the steady state.

2. Materials and Methods

2.1 Materials

Iridium wire ($\emptyset 0.30 \text{ mm} \times 100 \text{ mm}$, 99.9% purity), gold wire ($\emptyset 0.60 \text{ mm} \times 1 \text{ m}$, 99.95% purity), and silver wire ($\emptyset 0.60 \text{ mm} \times 1 \text{ m}$, 99.99% purity) were purchased from Nilaco, Japan. Li₂CO₃ (anhydrous powder, 99.9% purity) was purchased from Wako Pure Chemical Industries, Japan. Standard pH solutions with pH 4, pH 7, and pH 9 (pH standard solution set 101-S) were purchased from Horiba, Japan. Ultrapure water (Milli-Q) was supplied by Merck Millipore, USA.

2.2 Comparison of Ir/IrOx pH sensor fabrication processes

The oxidization of the iridium wires was conducted as described previously.⁽²²⁾ Briefly, iridium wire (5 mm long and 0.3 mm diameter) and gold wire (15 mm long and 0.6 mm diameter) were welded with a piezo gas burner. The welded wires were then cleaned using an ultrasonication bath containing acetone followed by ethanol and ultrapure water. After cleaning, the wires were dried in air. The wires were aligned on a gold sheet that covered an alumina crucible. Then, the wires were covered with excess Li_2CO_3 powder. On the basis of the original melt carbonate method, the wires were oxidized at 870 °C for 5 h and incubated at 120 °C overnight. To study the effect of fabrication factors, the oxidization temperature was varied from 750 to 950 °C at a constant oxidization time (Condition 1) or the oxidization time was varied from 1 to 6 h at a constant oxidization temperature (Condition 2). The wires were

oxidized in air inside an electric furnace. After cooling the wires to room temperature, the oxidized wires were rinsed with ultrapure water to dissolve the remaining crystallized Li_2CO_3 . The time necessary for the cleaning process depended on the amount of leftover Li_2CO_3 . After the oxidization process, we investigated the effect of annealing. The annealing process was conducted at 120 °C in an incubator overnight, whereas the nonannealing process was performed with the sensor in air. Table 1 summarizes the experimental conditions.

2.3 Characterization of pH sensor

To characterize the pH sensor, the open-circuit potential between the pH sensor and the Ag/ AgCl reference electrode was measured in a standard pH solution with a Keithley 6514 system electrometer and recorded using the LabVIEW data logging application. Figure 1 illustrates the measurement system. The potential data over time were then calculated for the pH responsivity and the drift potential.

Table 1

Conditions of three parameters in the fabrication processes: oxidization temperature, oxidization time, and annealing process.

Condition	Oxidization temperature (°C)	Oxidization time	Annealing process With annealing	
Original melt carbonate	870	(h) 5		
(Condition 1)	750		0	
Varied temperature,	800	Fixed at 5	With annealing	
constant time	950			
		1	With annealing	
		2		
(Condition 2)	$\Gamma' = 1 + 750$	3		
Varied time, constant temperature	Fixed at 750	4		
		5		
		6		
(0 1' 2)	750			
(Condition 3) Excluding annealing process	800	Fixed at 5	Without annealing	
	950			

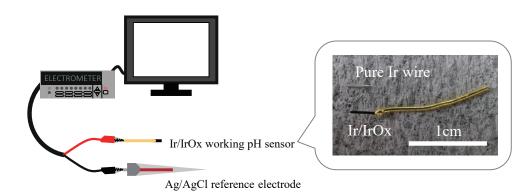


Fig. 1. (Color online) Setup of the open-circuit measurement consisting of an Ir/IrOx working pH sensor, Ag/ AgCl reference electrode, electrometer, and personal computer with a data logging application. The photograph shows the Ir/IrOx pH sensor and pure Ir prior to oxidization.

In detail, the pH responsivity was calculated by averaging the monitoring potential for the last 5 min in each pH step response. The averaging potential data sets were plotted against pH. Then, we estimated the slope using linear regression of 3 data points in the pH range 4 to 9, or 11 data points in the pH range 2 to 12. Drift potentials were calculated from the absolute value of the difference between averaged values of 5 and 10 min of each pH step response. The sensor performance and stability improved after several days. The initial pH responsivity was measured and calculated after the fabrication process was completed. Next, we measured the responsivity of the sensor for several days until the responsivity no longer changed. Then we determined the steady-state pH responsivity and the time required to reach the steady state. The initial potential drift and steady potential drift are defined as the value of drift taken immediately after fabrication and that taken several days after fabrication, respectively. The proton selectivity was evaluated under the addition of 0.1 M NaCl to the standard pH solution. The potential value was recorded in the above manner. The physical properties of the pH sensor were observed using a scanning electron microscope (SEM) (SU8240, Hitachi High-Technologies Corporation, Japan). The cross-sectioning of the pH sensor was performed via rough polishing, fine polishing, and ion milling.

3. Results and Discussion

3.1 Characterization of Ir/IrOx electrode

The electrochemical characteristics of the sensors were evaluated from the pH responsivity data. Two sensors were evaluated for each condition. Typical raw data of the open-circuit potential are shown in Fig. 2(a). The pH responsivity was calculated from the third cycle of raw data. The calculated pH response of the sensor is shown in Fig. 2(b). Nernst's equation is expressed as

$$E = E_0 - 2.303 \frac{RT}{nF} \log H^+, \tag{1}$$

where E is the electrode potential, E_0 is the standard potential, R is the universal gas constant, T is the absolute temperature, n is the electron activity, and F is Faraday's constant.

When T is 25 °C, the theoretical value of the pH responsivity is -59.2 mV/pH. Thus, the slopes of the linear functions on varied proton concentrations were evaluated and compared as pH responsivity. One of the advantages of the Ir/IrOx pH sensor is the proton selectivity. The sensor can neglect the effect of cationic species, and sense only proton activity in solution. The potentiometric response data in Figs. 2(c) and 2(d) showed no difference between with and without the addition of NaCl.

Thermal oxidization obviously changed the iridium portion of the sensor from silver to dark black. The surface morphology of sensors was investigated by SEM (Fig. 3). The Ir/IrOx sample shown in the figure was fabricated at an oxidization temperature of 870 °C, an oxidization time of 5 h, and an annealing time of 12 h. The SEM image of the sensor tip shows

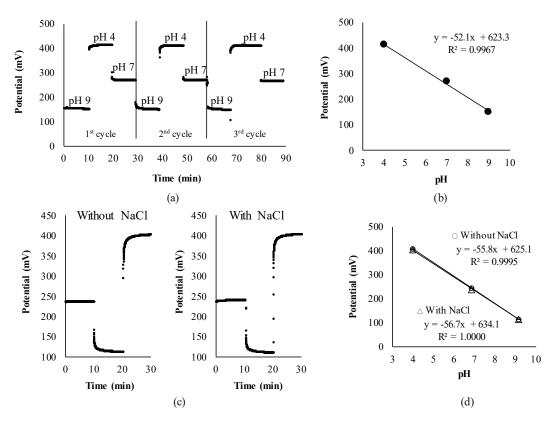


Fig. 2. Acquiring potential data and evaluation of pH responsivity: potential responses of the Ir/IrOx pH sensor as a function of (a) time and (b) pH in the stable state. Potential responses with and without 0.1 M NaCl as a function of (c) time and (d) pH.

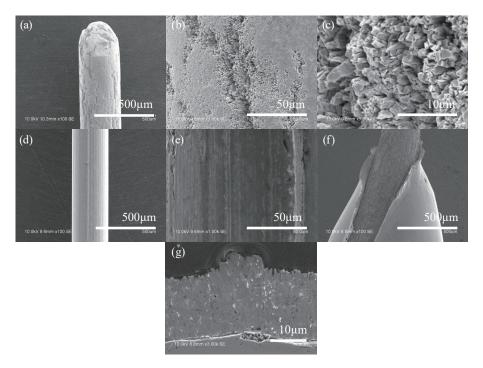


Fig. 3. High-magnification SEM images of the fabricated Ir/IrOx pH sensors: (a, b, c) IrOx tip, (d, e) pure Ir wire, (f) IrOx/Au junction, and (g) cross section of IrOx.

that the roughness on the whole surface area [Fig. 3(a)] differs from that of the bare iridium surface [Figs. 3(d) and 3(e)]. Additionally, the size and the density of the grains at the surface are nonuniformly distributed; some areas have small pores among the dense oxide surface. The holes of the nonuniform dense surface, which can be seen in Fig. 3(b), show the angular shape of the structure. Figure 3(c) shows the randomness of the grain size on the IrOx surface.

The changes in the surface morphology confirm that the oxide layer is successfully formed around the iridium core. Close-up SEM images of the IrOx/Au junction are shown in Fig. 3(f). The difference in the surface between IrOx and gold reveals that gold is inert to the melt-carbonate thermal oxidization. Figure 3(g) shows cross sections of the sensor. The oxide layer is clearly distinguished from the core iridium wire. The oxide thickness is approximately 20 μ m [Fig. 3(g)].

3.2 Effect of oxidization temperature

We investigated the effect of the oxidization temperature on the performance of the sensor (Table 2). We varied the oxidization temperature from 750 °C, which is the melting temperature of Li_2CO_3 , to 950 °C. The initial pH responsivity of each condition was not close to the theoretical value. The closest value was -43.8 mV/pH at a 750 °C oxidization temperature.

The raw data of the potentiometric response several days after fabrication are shown in Fig. 4(a); the acquiring potential data were unstable. There are potential shifts at each pH

Table 2

Initial pH responsivity, steady pH responsivity, and number of days from the initial to the steady state as a function of oxidization temperature with a 5 h oxidization time (Condition 1 in Table 1).

Oxidization	Initial pH	Steady pH	Number of days from
temperature (°C)	responsivity (mV/pH)	responsivity (mV/pH)	initial to steady state
750	-43.8	-55.7	3
800	-41.7	-55.5	11
870	-34.8	-49.1	14
950	-43.6	-55.6	17

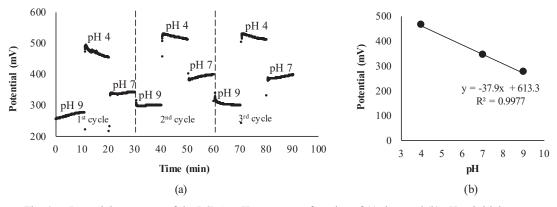


Fig. 4. Potential responses of the Ir/IrOx pH sensor as a function of (a) time and (b) pH at initial state.

value among every period. Furthermore, the pH responsivity [Fig. 4(b)] was different from that of the ideal pH sensor. However, after several days, the pH responsivity improved and approached the ideal responsivity; the value closest to the ideal one was -55.7 mV/pH at a 750 °C oxidization temperature. In some cases, the pH responsivity plateaued and did not show further improvement, regardless of the passage of time. The pH responsivity at an 870 °C oxidization temperature improved from -34.8 and reached a steady state at -49.1 mV/pH.

The time required for the sensor to reach the steady state was dependent on the conditions. For the 750 °C condition, the shortest time required was three days. Other conditions needed more than 10 days to reach the steady state. After the oxidization process, the pH responsivity improved to approximately -10 mV/pH and reached a stable value.

The drift potentials of each pH are shown in Table 3. Among the different oxidization temperatures, the 750 °C condition showed the lowest potential drift for almost all pH values in both the initial state and the steady state. In general, every condition showed an improved drift potential after the days passed. Normally, the drift potential phenomenon originates from the transition state from IrOx to IrO(OH) + H⁺ + e⁻, when the sensor surface is in contact with the aqueous solution phase.⁽²³⁾ We thought that it would take some time to reach equilibrium between IrOx and IrO(OH) at the surface. Once the surface of the sensor reaches electrochemical equilibrium, the potential of the sensor becomes stable, while drift of the potential occurs in the middle of the conditioning process before equilibrium.

3.3 Effect of oxidization time

Next, we investigated the oxidization time (Table 4). In the comparative study, we used an oxidization temperature of 750 °C, which is the most stable condition, as described in Sect. 3.2. Specifically, we compared the pH responsivity within three days of fabrication.

The pH responsivities after an oxidization time of 3 h were the closest to the ideal condition. The slopes for the two samples were -57.5 and -58.4 mV/pH. At 2 h, the samples also showed

Tal	bl	e	3
14	~	~	-

(,	1		
Oxidization		Initial potential drift (mV/min)		Steady potential drift (mV/min)	
	pH value				
temperature (°C)	_	1st sample	2nd sample	1st sample	2nd sample
870		4.7 ± 0.2	_	0.9 ± 0.6	
750	4	2.2 ± 0.5	0.5 ± 0.5	0.4 ± 0.1	0.2 ± 0.0
800	4	7.7 ± 1.2	4.0 ± 2.8	2.4 ± 2.9	0.2 ± 0.3
950		3.4 ± 1.1	4.1 ± 2.1	0.8 ± 0.5	0.5 ± 0.3
870		2.2 ± 0.2		0.6 ± 0.4	
750	7	0.6 ± 0.5	2.5 ± 2.9	0.3 ± 0.0	0.1 ± 0.1
800	7	3.2 ± 1.1	2.7 ± 2.1	0.8 ± 1.0	0.4 ± 0.1
950		2.4 ± 0.3	2.1 ± 1.4	0.4 ± 0.1	0.3 ± 0.3
870		1.3 ± 0.7		0.7 ± 0.3	
750	0	1.3 ± 1.4	2.1 ± 2.9	0.4 ± 0.1	0.4 ± 0.0
800	9	3.0 ± 2.9	0.8 ± 0.8	2.1 ± 0.6	0.8 ± 0.5
950		2.8 ± 1.3	0.7 ± 0.6	0.4 ± 0.5	0.9 ± 0.4

Initial and steady potential drift at different pH values as a function of oxidization temperature with a 5 h oxidization time (Condition 1 in Table 1). Two sensor samples were used for each condition.

pH responsivities after three days of oxidation as a function of oxidization time at a constant oxidization temperature of 750 $^{\circ}$ C (Condition 2 in Table 1). Two sensor samples were used for each condition.

Oxidization	pH responsivity (mV/pH)			
time (h)	1st sample	2nd sample		
1	-41.0 ± 5.0	-49.8 ± 2.0		
2	-54.0 ± 3.5	-53.4 ± 0.8		
3	-57.5 ± 1.0	-58.4 ± 0.9		
4	-41.2 ± 2.9	-55.3 ± 1.2		
5	-43.5 ± 1.2	-44.6 ± 1.8		
6	-47.0 ± 4.3	-47.9 ± 3.8		

-54.0 and -53.4 mV/pH, which are also close to the theoretical value. In the 4 h oxidization, one of the samples showed good pH responsivity, which is considered to be a result of the improvement of the fabrication process. As seen in the potential drift data (Table 5), an oxidization time of 3 h showed the smallest magnitude of the potential drift, which was almost zero under all conditions. The 2 h condition also showed small drift potential for most of pH values. One sample of 4 h oxidization showed low drift potential at every pH value, which supported the improvement. The characteristics of the sensors were not determined after an oxidization time of 1 h, as we assumed that this was an insufficient reaction time to form a complete thick and dense oxide layer.

Among the different oxidization times, the 3 h condition showed the optimum pH responsivity and the lowest potential drift for all pH values in the two samples with the initial state and the steady state. The 2 h condition also showed the small potential drift but not as well as the 3 h condition. That of the 4 h condition also showed further improvement. However, another sample of the 4 h condition did not meet the requirement of both pH responsivity and potential drift to give a better yield effect than those of 2 and 3 h. A reliable fabrication method that results in a better time effect would be worthwhile.

3.4 Effect of annealing process

After determining the optimum condition for the oxidization process, we evaluated the impact of the postfabrication process. Specifically, we investigated the effect of annealing at 120 °C after oxidization. Table 6 shows the difference in pH responsivity with and without the postannealing process. Overall, the nonannealing group showed a pH responsivity closer to the theoretical value. Table 7 shows the impact of annealing on drift potentials. Although there was a large variation in drift potentials between samples, the differences between the two conditions were very small. These results indicate that the postannealing process is unnecessary. After all the parameters were determined, the wide range of the pH responsivity from 2 to 12 was confirmed to ensure the linear response. The potentiometric reading of 11 pH values is shown in Fig. 5(a). The pH responsivity calculated from the linear regression of 11 points of pH is -57.1 mV/pH, as displayed in Fig. 5(b). Considering the calibration curves under the stable condition, the linearity and the fitting regression coefficient (R^2) are 0.9990 to 1.0000.

1		<	,	
Oxidization	pH value -	Potential drift (mV/min)		
time (h)	pri value	1st sample	2nd sample	
1		3.3 ± 1.0	1.8 ± 0.1	
2		0.9 ± 0.9	0.3 ± 0.2	
3	4	0.2 ± 0.2	0.3 ± 0.1	
4	4	2.1 ± 0.7	0.2 ± 0.1	
5		2.3 ± 0.5	0.5 ± 0.5	
6		1.3 ± 0.6	2.5 ± 1.1	
1		1.2 ± 0.9	0.3 ± 0.2	
2	7	0.7 ± 0.3	0.3 ± 0.2	
3		0.1 ± 0.0	0.0 ± 0.0	
4		1.3 ± 0.5	0.3 ± 0.2	
5		0.7 ± 0.5	2.5 ± 2.9	
6		0.9 ± 0.3	1.3 ± 1.7	
1		0.7 ± 0.1	0.5 ± 0.0	
2		1.3 ± 1.0	0.2 ± 0.2	
3	0	0.3 ± 0.2	0.1 ± 0.1	
4	9	0.8 ± 0.9	0.7 ± 0.5	
5		1.3 ± 1.4	2.1 ± 2.9	
6		0.8 ± 0.2	1.4 ± 1.4	

Table 5

Potential drift after three days of oxidation at different pH values as a function of oxidization time at a constant oxidation temperature of 750 °C (Condition 2 in Table 1). Two sensor samples were used for each condition.

Table 6

Effects of the postfabrication process (annealing vs nonannealing) on pH responsivity after three days of oxidization at different pH values as a function of oxidization temperature with a 5 h oxidization time (Condition 3 in Table 1). Two sensor samples were used for each condition.

Oxidization	1 1	onsivity	pH responsivity	
temperature (°C)	with annealing (mV/pH)		with nonannealing (mV/pH)	
temperature (C)	1st sample	2nd sample	1st sample	2nd sample
870 (control)	-28.0 ± 6.7			_
750	-43.5 ± 1.2	-55.1 ± 1.8	-53.2 ± 2.1	-51.0 ± 2.5
800	-33.3 ± 9.5	-44.0 ± 3.8	-45.3 ± 2.9	-43.3 ± 2.3
950	-33.0 ± 10.3	-39.6 ± 13.6	-45.8 ± 8.4	-48.8 ± 2.7

Table 7

Effects of the postfabrication process (annealing vs nonannealing) on potential drift after three days of oxidization at different pH values as a function of oxidization temperature with a 5 h oxidization time (Condition 3 in Table 1). Two sensor samples were used for each condition.

Oxidization		Potential drift		Potential drift	
	pH value	with annealing (mV/min)		with nonannealing (mV/min)	
temperature (°C)		1st sample	2nd sample	1st sample	2nd sample
870		4.7 ± 0.2			
750	4	2.2 ± 0.5	0.5 ± 0.5	1.6 ± 0.7	1.5 ± 0.7
800	4	7.7 ± 1.2	4.0 ± 2.8	2.6 ± 3.1	0.7 ± 0.3
950		3.4 ± 1.1	4.1 ± 2.1	7.2 ± 3.7	6.4 ± 5.9
870	7	2.2 ± 0.2			
750		0.6 ± 0.5	2.5 ± 2.9	1.0 ± 0.7	0.7 ± 0.5
800		3.2 ± 1.1	2.7 ± 2.1	1.4 ± 0.6	0.7 ± 0.2
950		2.4 ± 0.3	2.1 ± 1.4	1.6 ± 1.9	0.9 ± 1.1
870	9	1.3 ± 0.7			
750		1.3 ± 1.4	2.1 ± 2.9	1.6 ± 0.4	1.8 ± 1.6
800		3.0 ± 2.9	0.8 ± 0.8	1.5 ± 0.3	1.0 ± 0.1
950		2.8 ± 1.3	0.7 ± 0.6	1.5 ± 1.1	1.3 ± 0.5

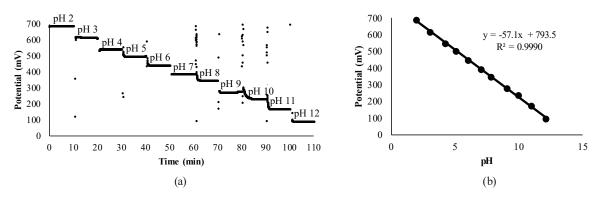


Fig. 5. Potential responses of 11 pH values from 2 to 12 of the 750 $^{\circ}$ C 3 h oxidization Ir/IrOx pH sensor as a function of (a) time and (b) 11 points pH calibration curve.

This study reveals that the Ir/IrOx fabrication process can be optimized by employing an oxidization temperature of 750 °C for 3 h without postannealing. The lower temperature and the shorter time should directly affect the thickness of the oxide layer. We assume that the thinner oxide layer would reach equilibrium at the surface more rapidly. These results indicate that the enhanced fabrication process not only has shorter fabrication time but also that less time is required for the sensor to reach a steady state. Beyond this fundamental study, further clinical studies should provide a better understanding toward acquiring robust pH measurements even in environments with many contaminants such as body fluid.

4. Conclusions

We successfully improved the sensor fabrication process by considering the fabrication temperature, the duration of the oxidization process, and the time required to reach the steady state. The optimum oxidization temperature in this study (750 °C) resulted in enhanced initial pH responsivity and the shortest time to reach the steady state. The optimum oxidization time was 3 h. Additionally, a postfabrication process was unnecessary since annealing did not improve sensor characteristics. This simplified oxidization method not only reduces the fabrication time but also enables reliable pH measurements.

Acknowledgments

This work was supported financially in part by the Center of Innovation Program from the Japan Science and Technology Agency, JST and the Ministry of Education, Culture, Sports, Science and Technology (MEXT) as part of the Research Center for Biomedical Engineering. The authors thank Professor Isamu Yuitoo of the Research Organization for Nano & Life Innovation, Waseda University.

References

- 1 S. Adler, A. Roy, and A. S. Relman: J. Clin. Invest. 44 (1965) 21.
- 2 H. J. Bright and M. Appleby: J. Biol. Chem. 244 (1969) 3625.
- 3 M. K. Weibel and H. J. Bright: J. Biol. Chem. 246 (1971) 2734.
- 4 L. Mu, I. A. Droujinine, N. K. Rajan, S. D. Sawtelle, and M. A. Reed: Nano Lett. 14 (2014) 5315.
- 5 R. Sahney, B. K. Puri, and S. Anand: Anal. Chim. Acta 542 (2005) 157.
- 6 R. Sahney, S. Anand, B. K. Puri, and A. K. Srivastava: Anal. Chim. Acta 578 (2006) 156.
- 7 C. S. Lee, S. K. Kim, and M. Kim: Sensors (Basel) 9 (2009) 7111.
- 8 W. Jin, L. Wu, Y. Song, J. Jiang, X. Zhu, D. Yang, and C. Bai: IEEE Trans. Biomed. Eng. 58 (2011) 1232.
- 9 W. Jin, J. Jiang, X. Wang, X. Zhu, G. Wang, Y. Song, and C. Bai: Respir. Physiol. Neurobiol. 177 (2011) 183.
- 10 S. Jamasb, S. Collins, and R. L. Smith: Sens. Actuators, B 49 (1998) 146.
- 11 J. C. Chou and C. N. Hsiao: Sens. Actuators, B 66 (2000) 181.
- 12 J. L. Chiang, S. S. Jan, J. C. Chou, and Y. C. Chen: Sens. Actuators, B 76 (2001) 624.
- 13 S. C. Mailley, M. Hyland, P. Mailley, J. M. McLaughlin, and E. T. McAdams: Mater. Sci. Eng. C 21 (2002) 167.
- 14 I. S. Lee, C. N. Whang, Y. H. Lee, G. Hwan Lee, B. J. Park, J. C. Park, W. S. Seo, and F. Z. Cui: Thin Solid Films 475 (2005) 332.
- 15 Y. Pan, T. Noda, K. Sasagawa, T. Tokuda, H. Kanda, T. Fujikado, and J. Ohta: J. Phys. Conf. Ser. 352 (2012) 012005.
- 16 T. Y. Kim and S. Yang: Sens. Actuators, B 196 (2014) 31.
- 17 J. Park, M. Kim, and S. Kim: Sens. Actuators, B 204 (2014) 197.
- 18 X. Huang, Q. Ren, X. Yuan, W. Wen, W. Chen, and D. Zhan: Electrochem. Commun. 40 (2014) 35.
- 19 S. Yao, M. Wang, and M. Madou: J. Electrochem. Soc. 148 (2001) H29.
- 20 W. D. Huang, H. Cao, S. Deb, M. Chiao, and J. C. Chiao: Sens. Actuators, A 169 (2011) 1.
- 21 R. Sheybani and A. Shukla: Biosens. Bioelectron .92 (2017) 425.
- 22 M. Wang, S. Yao, and M. Madou: Sens. Actuators, B 81 (2002) 313.
- 23 W. Olthuis, M. A. M. Robben, P. Bergveld, M. Bos, and W. E. van der Linden: Sens. Actuators, B 2 (1990) 247.